

MATERIALS SCIENCE

MRI-safe fiber electrodes for neuromodulation in the deep brain

Guo Tang and Xing Sheng 

Electrical neuromodulation including deep brain stimulation (DBS) treats intractable neurological and psychiatric disorders such as Parkinson's disease and autism spectrum disorder (ASD) [1–3]. Unraveling stimulation-evoked whole-brain circuits demands synchronized electrophysiology and multimodal magnetic resonance imaging (MRI) readout, a combination blocked by conventional implantable electrodes [4]. Clinically used platinum-iridium (PtIr) probes induce severe MRI artifacts via magnetic susceptibility mismatch and cause chronic brain inflammation due to extreme mechanical mismatch with soft neural tissue, leading to unstable long-term recording signals [1,5].

Previously developed carbon-based graphene fiber electrodes relieve partial imaging interference [6], yet they only operated below 9.4 T and did not integrate functional MRI (fMRI), diffusion-weighted imaging (DWI), and magnetic resonance spectroscopy (MRS) for deep-brain analysis [5–7]. Other soft polymer electrodes are limited to superficial cortical implantation and cannot support deep multimodal detection [4,8]. Furthermore, no existing device enables concurrent stimulation, electrophysiology, and multiparametric MRI at a high magnetic field of 11.7 T, restricting mechanistic research of deep neuromodulation [4,9].

In a recent study, Peng and co-workers report a structurally optimized MRI-compatible fiber neural electrode (MFE) based on a poly(3,4-ethylenedioxythiophene) polystyrene sulfonate (PEDOT:PSS) conduc-

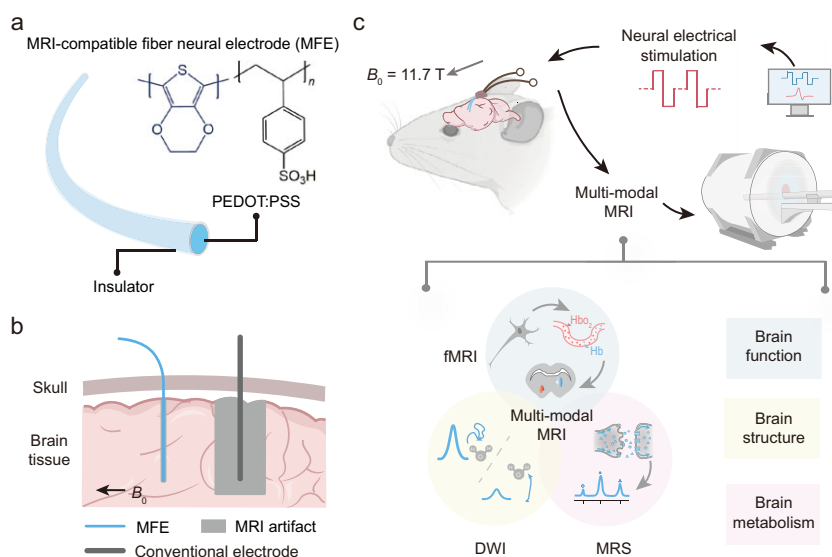


Figure 1. Multimodal investigation of neural modulation mechanisms with MFEs. (a) Schematic illustration of the MFE based on PEDOT:PSS. (b) Schematic illustration of the MRI artifacts induced by an MFE and a conventional MRI-incompatible neural electrode. (c) Schematic illustrating multimodal investigation of neuromodulation mechanisms through electrical stimulation synchronized with multimodal MRI, including fMRI, DWI, and MRS at 11.7 T. Reproduced from ref. [10] with permission.

tive polymer gel (Fig. 1a), which closely matches the magnetic susceptibility (-9.23 ppm) of brain tissue (-9.05 ppm) and delivers ultralow Young's modulus (328 kPa) far superior to all prior MRI-compatible neural probes [10]. At an 11.7 T ultrahigh field, MFEs produce negligible signal loss and artifact pixels ~ 10 -fold smaller than PtIr counterparts across 20–80 μm diameters (Fig. 1b), with minimal long-term implantation inflammation and radiofrequency heating risk. Electrochemically, the porous fiber architecture endows MFEs with two orders-of-magnitude higher charge injection limit (14.3 mC cm^{-2})

and far lower interfacial impedance, supporting high-fidelity single-unit recording and spatially precise localized stimulation.

Integrating MFEs into flexible chronic neural interfaces, the team realized simultaneous medial prefrontal cortex (mPFC) electrical stimulation, local field potential recording, and triple-modal MRI scanning in wild-type and MECP2-duplication autism model rats (Fig. 1c). Frequency-dependent whole-brain mapping revealed that high-frequency (130 Hz) mPFC stimulation reverses pathological functional and microstructural aberrations across autism-associated brain

regions, alongside distinct metabolic shifts in glutamate and taurine.

In sum, the MFE platform removes the long-standing technical bottleneck separating electrophysiological neuromodulation and ultrahigh-field multimodal MRI, constructing a universal analytical toolkit for dissecting whole-brain circuit dynamics. Looking ahead, this soft fiber bioelectronics holds promising translational prospects for human DBS clinical practice [1]. Real-time intra-operative MRI navigation with artifact-free electrodes will allow precise target localization for ASD, depression, and movement disorder treatments, while chronic post-implant MRI follow-up can dynamically track long-term circuit remodeling induced by stimulation [2,7]. Nevertheless, several translational

hurdles remain unresolved: scalable microarray fabrication for multiregion parallel recording, long-term biostability in human cerebrospinal fluid, and optimized packaging compatible with clinical 3 T/7 T MRI scanners. Further material modification and system miniaturization of PEDOT:PSS fiber electrodes will bridge the gap between rodent laboratory research and human clinical neuromodulation therapies, advancing personalized, mechanism-guided brain intervention [8,9].

Conflict of interest statement. None declared.

Guo Tang and Xing Sheng  *
Department of Electronic Engineering,
IDG/McGovern Institute for Brain Research,
Tsinghua University, China

*Corresponding author. E-mail:
xingsheng@tsinghua.edu.cn

REFERENCES

1. Coffey RJ. *Artif Organs* 2009; **33**: 208–20.
2. Zhang Y, Le S, Li H et al. *Biosens Bioelectron* 2021; **194**: 113592.
3. Xu M, Qi S, Calhoun V et al. *Neurobiol Dis* 2022; **173**: 105838.
4. Cho YU, Kim K, Dutta A et al. *Adv Funct Mater* 2024; **34**: 2310908.
5. Lu L, Fu X, Liew Y et al. *Nano Lett* 2019; **19**: 1577–86.
6. Zhao S, Li G, Tong C et al. *Nat Commun* 2020; **11**: 1788.
7. Dunn JF, Tuor UI, Kmech J et al. *Magn Reson Med* 2009; **61**: 222–8.
8. Liu Y, Li J, Song S et al. *Nat Biotechnol* 2020; **38**: 1031–6.
9. Gou S, Li P, Yang S et al. *Adv Funct Mater* 2025; **35**: 2570116.
10. Li W, Li X, Yang H et al. *Natl Sci Rev* 2026; **13**: nwag325.